Permanent Cardiac Pacing in Children: Choosing the Optimal Pacing Site: A Multicenter Study

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Permanent Cardiac Pacing in Children: Choosing the Optimal Pacing Site
A Multicenter Study

Jan Janoušek, MD, PhD; Irene E. van Geldorp, MD; Sylvia Krupičková, MD, PhD; Eric Rosenthal, MD; Kelly Nugent, BSc; Maren Tomaske, MD; Andreas Früh, MD; Jan Elders, RN, MA; Anita Hiippala, MD; Gunter Kerst, MD; Roman A. Gebauer, MD; Peter Kubuš, MD; Patrick Frias, MD; Fulvio Gabbarini, MD; Sally-Ann Clur, MBBCh, MSc, FCP(SA)Paed, PhD; Bert Nagel, MD; Javier Ganame, MD; John Papagiannis, MD, PhD; Jan Marek, MD; Svjetlana Tisma-Dupanovic, MD; Sabrina Tsao, MD; Jan-Hendrik Nürnberg, MD; Christopher Wren, MD; Mark Friedberg, MD; Maxime de Guillebon, MD; Julia Volkaufova, PhD; Frits W. Prinzen, MD, PhD; Tammo Delhaas, MD, PhD; for the Working Group for Cardiac Dysrhythmias and Electrophysiology of the Association for European Pediatric Cardiology

Background—We evaluated the effects of the site of ventricular pacing on left ventricular (LV) synchrony and function in children requiring permanent pacing.

Methods and Results—One hundred seventy-eight children (aged <18 years) from 21 centers with atrioventricular block and a structurally normal heart undergoing permanent pacing were studied cross-sectionally. Median age at evaluation was 11.2 (interquartile range, 6.3–15.0) years. Median pacing duration was 5.4 (interquartile range, 3.1–8.8) years. Pacing sites were the free wall of the right ventricular (RV) outflow tract (n=8), lateral RV (n=44), RV apex (n=61), RV septum (n=29), LV apex (n=12), LV midlateral wall (n=17), and LV base (n=7). LV synchrony, pump function, and contraction efficiency were significantly affected by pacing site and were superior in children paced at the LV apex/LV midlateral wall. LV dysynchrony correlated inversely with LV ejection fraction (R=0.80, P=0.0031). Pacing from the RV outflow tract/lateral RV predicted significantly decreased LV function (LV ejection fraction <45%; odds ratio, 10.72; confidence interval, 2.07–55.60; P=0.005), whereas LV apex/LV midlateral wall pacing was associated with preserved LV function (LV ejection fraction ≥55%; odds ratio, 8.26; confidence interval, 1.46–47.62; P=0.018). Presence of maternal autoantibodies, gender, age at implantation, duration of pacing, DDD mode, and QRS duration had no significant impact on LV ejection fraction.

Conclusions—The site of ventricular pacing has a major impact on LV mechanical synchrony, efficiency, and pump function in children who require lifelong pacing. Of the sites studied, LV apex/LV midlateral wall pacing has the greatest potential to prevent pacing-induced reduction of cardiac pump function. (Circulation. 2013;127:613-623.)

Key Words: heart block ■ heart failure ■ pacemakers ■ pacing ■ pediatrics

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From the Children’s Heart Center, University Hospital Motol, Prague, Czech Republic (J.J., S.K., P.K.); Department of Pediatric Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University Medical Center, Maastricht, Netherlands (J.E.v.G.); Evelina Children’s Hospital, London, United Kingdom (E.R., K.N.); University Children’s Hospital, Zurich, Switzerland (M.T.); Oslo University Hospital, Oslo, Norway (A.F.); Department of Cardiology, UMC St. Radboud, Nijmegen, Netherlands (J.E.); Department of Pediatric Cardiology, Children’s Hospital, University of Helsinki and Helsinki University Central Hospital, Helsinki, Finland (A.H.); Pädiatrische Kardiologie, Universitätsklinik für Kindermedizin und Jugendmedizin, Tübingen, Germany (G.K.); Department of Pediatric Cardiology, University of Leipzig, Heart Centre, Leipzig, Germany (R.A.G.); Department of Pediatric Cardiology, Children’s Hospital of Atlanta, Atlanta, GA (P.F.); Pediatric Cardiology Division, Children’s Hospital Regina Margherita, Turin, Italy (F.G.); Emma Children’s Hospital, Academic Medical Center, Amsterdam, and Center for Congenital Heart Anomalies Amsterdam/Leiden, Leiden, Netherlands (S.C.); Division of Pediatric Cardiology, Children’s Hospital, Medical University Graz, Graz, Austria (B.N.); Department of Pediatric Cardiology, University Hospital Leuven, Leuven, Belgium (J.G.); Division of Pediatric Cardiology, Mitera Children’s Hospital, Maroussi, Greece (J.P.); Department of Pediatric Cardiology, Great Ormond Street Hospital, London, United Kingdom (J.M.); Cardiology Section, Children’s Mercy Hospitals and Clinics, Kansas City, MO (S.T.-D.); Division of Cardiology, Children’s Memorial Hospital, Chicago, IL (S.T.); Klinikum Links der Weser, Abt Pediatric Cardiology, Bremen, Germany (J.N.); Department of Pediatric Cardiology, The Newscastle upon Tyne Hospitals, National Health Service Foundation Trust, Newcastle upon Tyne, United Kingdom (C.W.); Division of Cardiology, The Hospital for Sick Children, Toronto, Ontario, Canada (M.F.); Department of Congenital Heart Disease, Hôpital Cardiologique du Haut-Lévêque, Bordeaux University Hospitals, Bordeaux-Pessac, France (M.d.G.); Biostatistics Program, Louisiana State University Health Sciences Center, School of Public Health, New Orleans, LA (J.V.); Department of Physiology, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands (F.W.P.); and Department of Biomedical Engineering, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands (T.D.).

Correspondence to Jan Janoušek, MD, PhD, Children’s Heart Center, University Hospital Motol, V Úvalu 84, 150 06 Prague 5, Czech Republic. E-mail jan.janousek@lfmotol.cuni.cz

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Right ventricular (RV) pacing has been used for decades in both adults and children. Recently, several large adult studies,\textsuperscript{1-3} smaller pediatric reports,\textsuperscript{4,7} and a larger pediatric survey\textsuperscript{8} have pointed toward the adverse effects of RV pacing. The incidence of left ventricular (LV) dysfunction in RV paced children ranged within a median follow-up of less than a decade from 6.0% to 13.4%.\textsuperscript{7} The impact of pacing-induced dyssynchrony may be especially important in children with a prospect of lifelong pacing that lasts for decades. This idea is furthered by findings that dysynchronous LV activation causes pathological remodeling and dysfunction.\textsuperscript{9} Pediatric pacemaker therapy represents an optimal model for the evaluation of the long-term effects of different pacing sites because, on the basis of surgical preferences and in contrast to adults, various pacing sites are used, including LV epicardial pacing. In small single-center reports\textsuperscript{10-14} and a larger retrospective survey,\textsuperscript{1} pacing from the LV apex or free wall was associated with better preservation of LV function. The purpose of the present multicenter study was to evaluate the influence of different ventricular pacing sites on long-term LV function in children with nonsurgical atrioventricular block and a structurally normal heart and to search for a mechanism for the difference in pump function between sites by measuring mechanical synchrony and efficiency in a cross-sectional echocardiographic evaluation.

**Clinical Perspective on p 623**

**Methods**

**Recruitment and Demography**

Patients were recruited from 21 centers providing pacemaker therapy for children (17 European and 4 North American) and had to fulfill the following inclusion criteria: presence of second- or third-degree atrioventricular block necessitating permanent cardiac pacing with >70% ventricular paced beats; age <18 years at the time of primary pacemaker implantation; absence of any but trivial structural heart disease and of any known systemic illness potentially influencing cardiac function; duration of pacing >1 year; and no change in the ventricular pacing site during the follow-up period. A total of 178 patients (female, 96; male, 82; complete atrioventricular block in 171) were included in the study, with a median age at pacemaker implantation of 3.2 years and interquartile range (IQR) of 0.2 to 7.0 years. Atrioventricular block was congenital in 138 patients and diagnosed later during childhood in the remaining 40. Maternal autoantibodies were present in 64 of the 138 mothers tested. Nine of the 178 patients had patent ductus arteriosus that was closed interventionally with the use of coils before (n=3), at the time of (n=3), or after (n=3) pacemaker implantation. The retrospectively gathered data additionally included demographic parameters, preimplantation LV size and function, New York Heart Association classification, and pacemaker implantation details (pacing site as recorded by the implanting physician; lead type [endocardial versus epicardial]; and initial pacing mode and its change during the follow-up period).

**Cross-sectional Evaluation**

After ethical approval by the hospital review committee and patient consent according to individual institutional guidelines were obtained, eligible patients were evaluated according to a prespecified protocol including New York Heart Association class assignment, 12-lead ECG, echocardiography, and, if not available in the patient files, a chest x-ray in the anteroposterior and lateral projections. The echocardiographic protocol consisted of the following: (1) 2-dimensional gray scale loops of the parasternal long-axis view, parasternal short-axis view (at the level of papillary muscles), and apical 4-chamber and 2-chamber views; 3 cardiac cycles were recorded in each view along with simultaneous ECG tracing to allow for identification of QRS onset; 3.5- and 5-MHz transducers with a minimal frame rate of 30 per second (ideally 60–90 per second) were used; (2) parasternal long-axis and short-axis M mode; and (3) pulsed Doppler of the RV outflow tract (RVOT) and LV outflow tract, pulsed transmitial Doppler, and qualitative assessment of mitral regurgitation (none=0, mild=1, moderate=2, and severe=3). Recordings were stored on CD/DVD as raw data from Vivid-GE systems and in Digital Imaging and Communications in Medicine format for other vendors.

**Data Analysis**

All data were analyzed in a core laboratory (Children’s Heart Center, Prague, Czech Republic). First, QRS duration was measured manually as the maximum value in any lead from ECG printouts with a sweep speed of 25 or 50 mm/s. Second, approximate pacing site assignment was performed with the use of 12-lead ECG QRS morphology and axis and biplane chest x-rays to allow grouping into 7 categories for the purpose of statistical evaluation: free wall of the RVOT, lateral RV wall, RV apex, RV septum (any position), LV apex, lateral LV wall, and LV base. We used published algorithms for exact differentiation of the RV septal sites from the RVOT free wall sites.\textsuperscript{15} Assignment to the RV lateral wall was performed in case of a leftward QRS axis along with left bundle-branch block morphology. RV and LV apical pacing were characterized by superior axis and left and right bundle-branch block morphology in lead I, respectively. Pacing was assigned to the LV lateral wall or LV base in case of a rightward QRS axis along with right bundle-branch block morphology with further differentiation according to the biplane x-ray. Third, the following echocardiographic analysis, measurements, and calculations were performed:

1. LV dimensions were measured from the parasternal long-axis M-mode and expressed as Z scores with the use of weight-related normal limits.\textsuperscript{16} LV shortening fraction was calculated.
2. LV volumes were measured from the apical 4- and 2-chamber views with the Simpson biplane method. LV ejection fraction (EF) was calculated and graded as follows: normal (LV EF ≥55%), subnormal (LV EF <55%), and significantly decreased (LV EF <45%).
3. Septal to posterior wall motion delay was measured from the parasternal short-axis M mode.\textsuperscript{17} When maximum systolic motion was unclear, maximum systolic wall thickening was taken as the maximal excursion.
4. Interventricular mechanical delay was calculated as the difference between LV and RV pre-ejection periods measured from QRS onset to the beginning of ventricular ejection with the use of pulsed Doppler from the RVOT and LV outflow tract.

Speckle tracking analysis was performed in 125 of 178 subjects with echocardiographic raw data available from Vivid-GE equipment (GE-Vingmed, Horten, Norway) with the use of an EchoPac workstation. Longitudinal segmental strain was calculated in the apical 4- and 2-chamber views and radial strain in the parasternal short-axis view according to standardized myocardial segmentation.\textsuperscript{18,19} Each of the 3 recorded cardiac cycles was inspected visually with examination of both strain rate and strain curves, and the one with the least strain rate noise and unequivocally identifiable strain peaks was used for measurement. Segments automatically rejected by the software or those with unclear peaks were not used for analysis. Measurements were feasible in 938 of 1380 segments (68.0%) in the apical views and 625 of 660 segments (94.7%) in the short-axis view. Peak segmental systolic deformation timing, defined as the time from QRS onset to peak systolic strain, was measured in each segment. Subsequently, mechanical delays were calculated as the median time between peak systolic strain, as follows: (1) septal to lateral delay from the basal segments of the apical 4-chamber view; (2) anterior to inferior delay from the basal segments of the apical 2-chamber view; and (3) septal to lateral, anterosepal to posterior, and anterior to inferior delays.
from the parasternal short-axis view. Furthermore, a modified strain dysynchrony index was calculated. This index reflects wasted segmental contraction due to LV dyssynchrony. In brief, the difference between maximum and end-systolic strain (at the time of aortic valve closure as indicated by the end of systolic flow in the LV outflow tract) was measured in each segment and expressed as percentage of the respective maximum segmental strain. The proportion of wasted LV contraction was then calculated separately for the RV and LV pacing sites from the 12 LV segments in the apical 4- and 2-chamber views (basal, mid, and apical levels) and from the 6 segments in the parasternal short-axis view, respectively, as the sum of the segmental values divided by the number of segments. Wasted energy can result from premature end of shortening (maximum falls before aortic valve closure, as occurs in early-activated regions) or from postsystolic shortening (as occurs in late-activated regions). To ensure correct delineation of aortic valve closure, measurements were rejected if the difference between the cardiac cycle length of the aortic outflow Doppler and the respective speckle tracking measurement was >10%.

### Statistical Analysis

If not otherwise stated, continuous data are presented as raw means (SDs). Differences in demographic and informative variables between pacing sites were evaluated by 1-way ANOVA with the use of the Holm-Sidak method for pairwise multiple comparisons or by the χ2 test, as appropriate. The continuous outcome variables characterizing LV function and synchrony were analyzed with the use of a linear mixed model approach. Each model included the set of clinically informative additive covariates in addition to the main factor tested. The continuous covariates included age at implantation, pacing duration, and QRS duration. The dichotomous covariates were gender, presence of maternal antibodies, presence of congenital block, and DDD pacing. The main treatment factor included was the pacing site with 7 levels or a combination of specific pacing sites. In all models, the class variable “contributing center” was included as an additive random effect. For the random center effect, a simple covariance structure was assumed in all models. The statistical test of main treatment effect was an adjusted F test with Kenward-Roger type adjustment of denominator degrees of freedom. For the “site” main effect, multiple comparisons were performed with the use of the

### Table 1. Demographic, Clinical, and Pacing Parameters According to Ventricular Pacing Site

<table>
<thead>
<tr>
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<th></th>
<th></th>
<th></th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>No. of patients</td>
<td>8</td>
<td>44</td>
<td>61</td>
<td>29</td>
<td>12</td>
<td>17</td>
<td>7</td>
<td>...</td>
<td>...</td>
</tr>
<tr>
<td>Male, n (%)</td>
<td>7 (87.5)</td>
<td>21 (47.7)</td>
<td>33 (54.1)</td>
<td>11 (37.9)</td>
<td>1 (8.3)</td>
<td>6 (35.3)</td>
<td>3 (42.9)</td>
<td>0.016</td>
<td>...</td>
</tr>
<tr>
<td>CCAVB, n (%)</td>
<td>6 (75.0)</td>
<td>35 (79.5)</td>
<td>47 (77.0)</td>
<td>20 (69.0)</td>
<td>9 (75.0)</td>
<td>16 (94.1)</td>
<td>5 (71.4)</td>
<td>0.467</td>
<td>...</td>
</tr>
<tr>
<td>Maternal antibodies, yes/no/unknown, n (%)</td>
<td>5/3/0</td>
<td>16/22/6</td>
<td>19/27/15</td>
<td>12/13/4</td>
<td>7/2/3</td>
<td>5/3/9</td>
<td>0/2/5</td>
<td>0.644</td>
<td>...</td>
</tr>
<tr>
<td>LVEDD before implantation, Z score</td>
<td>1.64 (1.06)</td>
<td>1.81 (1.79)</td>
<td>1.79 (1.74)</td>
<td>2.11 (1.96)</td>
<td>1.71 (2.13)</td>
<td>1.49 (0.86)</td>
<td>1.53 (1.98)</td>
<td>0.980</td>
<td>...</td>
</tr>
<tr>
<td>LVSF before implantation, n (%)</td>
<td>42 (5)</td>
<td>38 (7)</td>
<td>41 (7)</td>
<td>43 (7)</td>
<td>40 (5)</td>
<td>42 (8)</td>
<td>41 (5)</td>
<td>0.359</td>
<td>...</td>
</tr>
<tr>
<td>LV EF before implantation, n (%)</td>
<td>65 (14)</td>
<td>66 (12)</td>
<td>62 (12)</td>
<td>61 (14)</td>
<td>68 (14)</td>
<td>60 (11)</td>
<td>64 (5)</td>
<td>0.632</td>
<td>...</td>
</tr>
<tr>
<td>Age at implantation, y</td>
<td>3.52 (5.61)</td>
<td>2.85 (3.64)</td>
<td>5.32 (4.29)</td>
<td>6.76 (5.43)</td>
<td>1.69 (2.50)</td>
<td>3.78 (4.61)</td>
<td>6.34 (6.32)</td>
<td>0.002</td>
<td>4 vs 2.5</td>
</tr>
<tr>
<td>Age at follow-up, y</td>
<td>7.02 (5.38)</td>
<td>9.73 (4.50)</td>
<td>12.62 (4.91)</td>
<td>12.78 (4.36)</td>
<td>4.08 (2.98)</td>
<td>10.08 (5.68)</td>
<td>11.72 (5.17)</td>
<td>&lt;0.001</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Duration of pacing, y</td>
<td>3.51 (1.77)</td>
<td>6.87 (3.85)</td>
<td>7.31 (4.25)</td>
<td>6.02 (4.21)</td>
<td>2.38 (0.97)</td>
<td>6.30 (4.02)</td>
<td>5.39 (3.84)</td>
<td>0.002</td>
<td>5 vs 2.3</td>
</tr>
<tr>
<td>DDD pacing at follow-up, n (%)</td>
<td>6 (75.0)</td>
<td>11 (25.0)</td>
<td>33 (54.1)</td>
<td>16 (55.2)</td>
<td>6 (50.0)</td>
<td>10 (58.8)</td>
<td>6 (85.7)</td>
<td>0.007</td>
<td>...</td>
</tr>
<tr>
<td>QRS duration at follow-up, ms</td>
<td>143 (13)</td>
<td>157 (20)</td>
<td>157 (21)</td>
<td>146 (19)</td>
<td>127 (23)</td>
<td>158 (25)</td>
<td>177 (22)</td>
<td>&lt;0.001</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>NYHA classification at follow-up</td>
<td>1.03 (0.17)</td>
<td>1.00 (0.00)</td>
<td>1.00 (0.00)</td>
<td>1.03 (0.19)</td>
<td>1.00 (0.00)</td>
<td>1.00 (0.00)</td>
<td>1.00 (0.00)</td>
<td>0.628</td>
<td>...</td>
</tr>
</tbody>
</table>

Data are presented as number (percentage) or mean (SD). Numbers in square brackets and in the P value column refer to pacing site categories. CCAVB indicates congenital complete atrioventricular block; LVEDD, left ventricular end-diastolic dimension; LV EF, left ventricular ejection fraction; LVSF, left ventricular shortening fraction; NYHA, New York Heart Association; and RVOT, free wall of the right ventricular outflow tract.
Tukey-Kramer adjustment. The 2 dichotomous variables calculated from LV EF with a cutting point of 45% and 55%, respectively, were analyzed by a generalized mixed linear model. The distribution of the response was set to be binomial, and the probability of LV EF <45% (≥55%) was modeled by a log-link function. The covariates and main treatment effects were the same as for continuous variables. The data for dichotomous response are presented as odds ratios (95% confidence intervals). The difference in the modified strain dyssynchrony index between RV and LV pacing was evaluated by the Mann-Whitney rank sum test. Correlation between 2 continuous variables was evaluated by linear regression. Interobserver variability was tested by the coefficient of variation.21 SigmaPlot for Windows.
LV shortening fraction, biplane EF, and the end-systolic volume index (both available in 157 of 178 patients) were different between pacing sites, whereas the Z score of the LV end-diastolic dimension and the end-diastolic volume index did not differ. LV apex and lateral LV wall pacing yielded significantly higher shortening fraction and EF than did RV pacing sites (Figure 2). LV EF was not significantly different between RV septum and RV apex pacing. Patients with RVOT and lateral RV wall pacing had the largest scatter in LV EF, with the lower quartile as low as <38% in the RVOT group (Figure 2B). Patients with subnormal LV EF (<55%) were almost exclusively confined to RV pacing sites or LV base pacing, whereas the vast majority of patients paced from the LV apex or lateral wall had completely preserved LV function (Figure 3). Compared with preimplantation values, the decrease in LV shortening fraction was significant for all RV pacing sites and absent in the LV paced groups (Figure 4). Comparison of the best and clinically most commonly used RV site (ie, RV apex) with the combination of optimal LV sites (LV apex and lateral LV wall) still yielded a significant difference in favor of LV pacing (Table 2). To elucidate the potential effect of maternal autoantibodies, presence of congenital atroventricular block, gender, age at implantation, pacing duration, DDD pacing, and QRS duration on LV function, these variables were introduced as covariates. Pacing site was the only significant predictor of both LV EF and shortening fraction (P<0.0001 for both), whereas none of the covariates reached significance. RVOT/lateral RV wall pacing was the only independent predictor of significantly decreased LV EF (<45%), whereas LV apex/lateral LV wall pacing was associated with preservation of LV function (LV EF ≥55%; Tables 3 and 4). To allow for comparison with a recent multicenter retrospective survey, we also analyzed LV function by whether subjects were RV epicardial, RV endocardial, or LV paced. Results were similar to the previous findings, with LV pacing being superior to RV endocardial or epicardial pacing in terms of LV shortening fraction, LV EF, and change in LV shortening fraction compared with preimplantation values (Table 5). No difference was found between RV apical epicardial and endocardial pacing.

**LV Dyssynchrony**

The interventricular and intra-LV delays were significantly different between pacing sites (Figure 5). LV EF and septal to posterior wall motion delay for the individual pacing sites are depicted in Figure 6. Segmental strain analysis by speckle tracking confirmed this mechanical dyssynchrony pattern (Figures 7, 8A, and 8B). RV pacing consistently produced delayed LV ejection and a mechanical contraction delay between the septum and LV free wall with the least negative effect of the RV outflow tract.

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**Table 2. Comparison of LV Function Between RV Apical and LV Apical Plus Lateral Wall Pacing**

<table>
<thead>
<tr>
<th>Pacing Site</th>
<th>RV Apex</th>
<th>LV Apex+Lateral</th>
<th>P</th>
</tr>
</thead>
<tbody>
<tr>
<td>n</td>
<td>61</td>
<td>29</td>
<td></td>
</tr>
<tr>
<td>LVSF, %</td>
<td>34 (7)</td>
<td>40 (6)</td>
<td>0.0007</td>
</tr>
<tr>
<td>Change in LVSF, U (compared</td>
<td>−7 (9)</td>
<td>−1 (9)</td>
<td>0.044</td>
</tr>
<tr>
<td>LV EF, %</td>
<td>54 (6)</td>
<td>61 (6)</td>
<td>0.0015</td>
</tr>
<tr>
<td>LVESVi, mL/m² BSA</td>
<td>29 (9)</td>
<td>21 (5)</td>
<td>0.260</td>
</tr>
</tbody>
</table>

Data are presented as mean (SD). BSA indicates body surface area; EF, ejection fraction; LV, left ventricular; LVESVi, LV end-systolic volume index; LVSF, LV shortening fraction; and RV, right ventricular.

---

**Table 3. Risk Factors for Decreased LV Function (LV EF <45%)**

<table>
<thead>
<tr>
<th>Variable in Model</th>
<th>LV EF &lt;45%</th>
<th>LV EF ≥45%</th>
<th>P</th>
<th>Odds Ratio (95% CI)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Male gender, %</td>
<td>50.0</td>
<td>45.4</td>
<td>0.810</td>
<td>0.83 (0.10–3.81)</td>
</tr>
<tr>
<td>Congenital atrioventricular block, %</td>
<td>75.0</td>
<td>77.5</td>
<td>0.783</td>
<td>0.72 (0.07–7.42)</td>
</tr>
<tr>
<td>Maternal autoantibodies, %</td>
<td>61.5</td>
<td>43.6</td>
<td>0.406</td>
<td>2.51 (0.28–22.35)</td>
</tr>
<tr>
<td>Age at implantation, y</td>
<td>4.39 (4.79)</td>
<td>4.49 (4.66)</td>
<td>0.592</td>
<td>0.93 (0.72–1.21)</td>
</tr>
<tr>
<td>RVOT and lateral RV wall pacing, %</td>
<td>62.5</td>
<td>24.8</td>
<td>0.005</td>
<td>10.72 (2.07–55.60)</td>
</tr>
<tr>
<td>DDD pacing, %</td>
<td>50.0</td>
<td>48.2</td>
<td>0.520</td>
<td>1.77 (0.31–10.25)</td>
</tr>
<tr>
<td>Pacing duration, y</td>
<td>4.94 (3.32)</td>
<td>6.44 (4.13)</td>
<td>0.115</td>
<td>0.60 (0.75–1.06)</td>
</tr>
<tr>
<td>QRS duration, ms</td>
<td>154 (26)</td>
<td>154 (22)</td>
<td>0.477</td>
<td>1.02 (0.97–1.07)</td>
</tr>
</tbody>
</table>

Data are presented as percentage or mean (SD). CI indicates confidence interval; EF, ejection fraction; LV, left ventricular; RV, right ventricular; and RVOT, free wall of the RV outflow tract.
QRS duration, ms 149 (22) 158 (23) 0.593 0.99 (0.97–1.02)
Pacing duration, y 5.88 (3.78) 6.64 (4.30) 0.425 0.95 (0.84–1.08)
DDD pacing, % 45.8 50.6 0.455 1.50 (0.52–4.33)
LV apical and lateral LV wall pacing, % 4.7 29.2 0.018 8.26 (1.46–47.62)
Age at implantation, y 4.24 (4.46) 4.69 (4.83) 0.323 0.94 (0.82–1.07)
Maternal autoantibodies, % 41.1 49.3 0.103 0.37 (0.11–1.23)
Congenital atrioventricular block, % 73.6 80.5 0.972 0.98 (0.29–3.35)

Contraction Efficiency
The proportion of wasted LV contraction due to dyssynchrony measured by a modification of the strain dyssynchrony index²⁰ was significantly higher during RV pacing than during LV pacing for both radial and longitudinal systolic function, as follows: median 8.3% (IQR, 5.7–14.5%) versus 3.1% (2.2–3.5%) (P<0.001) and 6.2% (IQR, 5.0–8.2%) versus 2.1% (1.2–3.5%) (P<0.001), respectively.

Interobserver agreement (J.J., I.E.v.G.) was calculated in a total of 28 of 178 patients. Pacing site assignment was equal in 27 of 28 patients. The following coefficients of variation²¹ were achieved in the parameters tested: biplane LV EF=9.7%, interventricular mechanical delay=5.7%, septal to posterior wall motion delay=11.2%, and intersegmental mechanical delay from 2-dimensional strain=0.9%.

Table 4. Factors Associated With Preserved LV Function (LV EF ≥55%)

<table>
<thead>
<tr>
<th>Variable in Model</th>
<th>LV EF ≥55%</th>
<th>LV EF &lt;55%</th>
<th>P</th>
<th>Odds Ratio (95% CI)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Male gender, %</td>
<td>36.1</td>
<td>54.1</td>
<td>0.086</td>
<td>0.45 (0.18–1.12)</td>
</tr>
<tr>
<td>Congenital atrioventricular block, %</td>
<td>73.6</td>
<td>80.5</td>
<td>0.972</td>
<td>0.98 (0.29–3.35)</td>
</tr>
<tr>
<td>Maternal autoantibodies, %</td>
<td>41.1</td>
<td>49.3</td>
<td>0.103</td>
<td>0.37 (0.11–1.23)</td>
</tr>
<tr>
<td>Age at implantation, y</td>
<td>4.24 (4.46)</td>
<td>4.69 (4.83)</td>
<td>0.425</td>
<td>1.50 (0.52–4.33)</td>
</tr>
<tr>
<td>LV apical and lateral LV wall pacing, %</td>
<td>4.7</td>
<td>29.2</td>
<td>0.018</td>
<td>8.26 (1.46–47.62)</td>
</tr>
<tr>
<td>DDD pacing, %</td>
<td>45.8</td>
<td>50.6</td>
<td>0.455</td>
<td>1.50 (0.52–4.33)</td>
</tr>
<tr>
<td>Pacing duration, y</td>
<td>5.88 (3.78)</td>
<td>6.64 (4.30)</td>
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</tr>
<tr>
<td>QRS duration, ms</td>
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<td>0.593</td>
<td>0.99 (0.97–1.02)</td>
</tr>
</tbody>
</table>

Table 5. Differences Between RV Epicardial, RV Endocardial, and LV Pacing

<table>
<thead>
<tr>
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<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>LVSF, %</td>
<td>31 (5)</td>
<td>33 (7)</td>
<td>40 (6)</td>
<td>&lt;0.0001</td>
<td>&lt;0.001, 1,2 vs 3</td>
</tr>
<tr>
<td>Change in LVSF, SF units</td>
<td>−8 (9)</td>
<td>−8 (9)</td>
<td>−1 (9)</td>
<td>0.023</td>
<td>0.0235, 2 vs 3</td>
</tr>
<tr>
<td>LV EF, %</td>
<td>52 (8)</td>
<td>53 (7)</td>
<td>60 (6)</td>
<td>&lt;0.0001</td>
<td>&lt;0.001, 1,2 vs 3</td>
</tr>
</tbody>
</table>

Data are presented as percentage or mean (SD). CI indicates confidence interval; EF, ejection fraction; and LV, left ventricular.

Discussion
This study strongly supports previous findings of a retrospective pediatric report showing a decrease in LV function specifically due to RV free wall pacing. Our results also confirm data on preservation of LV function with LV apical or LV lateral wall pacing,²⁰-²⁴ including a large retrospective pediatric multicenter survey⁴ and a recently published experimental study.²² Our present report does not show any superiority of RV septal over RV apical pacing. This is in agreement with another experimental work published by Mills et al a few years ago. Some clinical studies showed promising results with the use of RV septal lead placement,²⁴ but clear benefit from RV septal pacing has not yet been demonstrated in a randomized trial, except when the lead is positioned in the His bundle.²⁵

RV pacing (in contrast to LV pacing) was associated with depressed systolic function and induced a consistent decrease in LV systolic function compared with preimplantation values. This decrease was functionally well tolerated because no difference in New York Heart Association class was observed between the pacing sites. However, given the cross-sectional design of the study, patients suffering from symptomatic heart disease. The results can be summarized as follows:

1. LV apical and LV lateral wall pacing are associated with the best preservation of LV function, which appears to be related to preserved mechanical synchrony and contraction efficiency.
2. RV pacing sites carry a high risk for a negative effect on LV performance, coinciding with significant mechanical asynchrony and contraction inefficiency. This effect is most pronounced for RV lateral and RVOT pacing and less pronounced for RV apical pacing.
3. Nontargeted RV septal pacing does not show any advantage over RV apical pacing.
4. LV basal pacing produces a significantly reversed pattern of LV dyssynchrony and should probably not be the preferred LV pacing site.
5. The presence of maternal autoantibodies is not associated with decreased LV function and could not be confirmed as a modifier of the response to pacing-induced LV dyssynchrony.
failure may have been missed because they were upgraded to a biventricular system, were transplanted, or died. The incidence of patients suffering from heart failure due to RV pacing has been reported to range from 6.0% to 13.4% in previous pediatric reports.\textsuperscript{5–7}

Results of this study further indicate that LV pacing may be a substitute for primary biventricular pacing, which has recently been shown to preserve LV function in chronically paced adults.\textsuperscript{20} As demonstrated by Tomaske et al\textsuperscript{27} and Vanagt et al\textsuperscript{28} in small descriptive pediatric reports, LV pacing may also be used instead of biventricular pacing to improve LV function that has been compromised from long-term RV pacing.

QRS duration was not a multivariable predictor of decreased LV function because it reflects the total electric activation time but not the sequence of activation. Recently, a subanalysis of

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**Figure 5.** A. Interventricular mechanical delay (IVMD). B. Septal to posterior wall motion delay (SPWMD). To allow for comparisons between pacing sites, statistical significance is calculated for absolute measurement values. Dotted line indicates interventricular/intraventricular synchrony. LVA indicates left ventricular apex; LVB, left ventricular base; LVLat, lateral left ventricular wall; RVA, right ventricular apex; RVLat, lateral right ventricular wall; RVOT, free wall of the right ventricular outflow tract; and RVS, right ventricular septum.

**Figure 6.** Approximate pacing sites as assessed from biplane chest x-rays and 12-lead ECG and color-coded absolute values of left ventricular (LV) ejection fraction (EF) (A) and septal to posterior wall motion delay (SPWMD) (B) in each specific patient. RV indicates right ventricle. Adapted with permission from Netter FH. Atlas of Human Anatomy. 2nd ed. Hansen JT, consulting ed. Teterboro, NJ: Icon Learning Systems; 1997; plates 205 and 213 (pacing sites are not part of the original image and were added by the authors).
the Multicenter Automatic Defibrillator Implantation Trial–Cardiac Resynchronization Therapy (MADIT-CRT) has shown that left bundle-branch block morphology rather than QRS duration is the prerequisite for the efficacy of cardiac resynchronization therapy. This implies that a specific activation pattern is more important than total asynchrony. Our study indicates that the negative effects of LV dyssynchrony produced by RV pacing are preventable by LV pacing irrespective of QRS duration.

The presence of maternal autoantibodies in the setting of congenital atrioventricular block was not found to be a component of individual reactivity to pacing-induced LV dyssynchrony as opposed to a study showing association of autoimmune atrioventricular block with dilated cardiomyopathy. None of the patients who were paced from the LV showed decreased LV function, despite the presence of maternal autoantibodies in a significant portion. RV pacing–induced LV dysfunction has been reported previously in the absence of maternal autoantibodies in children with surgical atrioventricular block and could be effectively corrected by an upgrade to biventricular pacing. All of these findings support our statement that the pacing site plays a crucial role in the development of pacing-associated LV dysfunction.

Figure 7. A, Mechanical activation pattern in right ventricular (RV) free wall pacing showing early peak negative 2-dimensional strain in the basal and midventricular septum (yellow arrow) and late negative strain peak in the left ventricular (LV) free wall (red arrow). An extensive septal to lateral mechanical dyssynchrony with a delay of 300 ms is present. B, LV apical pacing with mechanical activation starting at the apex (yellow arrows) and proceeding to the base (red arrows), resulting in almost complete septal to lateral mechanical synchrony.
Study Limitations
This study has limitations related to the unequal number of patients in each pacing site group, significant differences in age at primary implantation, and duration of pacing, as well as the accuracy of the retrospective assessment of the pacing site with the use of surgical records, biplane x-ray, and 12-lead ECG. However, neither age nor duration of pacing was a multivariable predictor of LV dysfunction, and pacing site localization could be performed with acceptable interobserver variability. In addition, there is some degree of uncertainty about the exact proportion of fully captured paced beats during the entire pacing period. However, the vast majority of patients had complete atrioventricular block (171/178) with a low probability of spontaneous rhythm. Moreover, all available 12-lead ECGs showed a permanently paced rhythm in all cases. The lack of atrioventricular synchrony as present in the patients with VVI(R) pacing may have been another confounder. The pacing mode was, however, not a factor influencing LV function in any of the analyses performed. Additionally, biplane LV EFs were not available in all patients. The differences between pacing sites, however, could be confirmed by the analysis of LV shortening fractions. In addition, the study protocol did not include RV evaluation, and potentially negative effects of LV pacing on RV function could therefore not be assessed. One of the legitimate statistical concerns is that a certain bias in the analysis of the mean response is introduced because the patients were not randomized with respect to pacing sites. However, in our approach we addressed this limitation by including all available confounders in all analyzed models as covariates. Propensity score adjustment might be considered an alternative approach. We have not applied it here because the basic assumption for the propensity score analysis, that no additional confounders exist other than those collected on patients, was not verifiable.

Conclusions
The site of ventricular pacing has a major impact on LV mechanical synchrony, efficiency, and pump function in children who require lifelong pacing. Of the sites evaluated in the present study, LV apex/lateral LV wall pacing has the greatest potential to prevent pacing-induced reduction of cardiac pump function, whereas RVOT/lateral RV wall pacing is associated with a high risk of LV dysfunction. Although it is associated with a mild decrease in LV EF in approximately one half of the patients, RV apex pacing is well tolerated in the majority. These data may guide clinicians in selecting proper pacing strategies in a population that will be subjected to several decades of permanent cardiac pacing and in which the aim to optimally preserve LV synchrony and function should be mandatory. Surgical access to the LV is possible with the use of existing tools and at no additional cost: the subxiphoid approach in younger children or, in older ones, a left lateral thoracotomy with an excellent cosmetic result.33 The results of the present study also provide an important clinical confirmation of previously published experimental research.22,23,34,35
Sources of Funding
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Disclosures
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References
Clinical Perspective

Permanent cardiac pacing that starts in childhood will continue for decades. The observed reduction in left ventricular (LV) function in right ventricular–paced children is only the beginning of a process that will likely develop further over subsequent decades. Thus, the aim to preserve LV synchrony and function should be mandatory. The site of ventricular pacing has a major impact on LV mechanical synchrony, efficiency, and pump function in children who require lifelong pacemaker therapy. These clinical findings have provided an important confirmation of previously published experimental research. Pediatric patients with a systemic LV who are scheduled for epicardial lead implantation should be paced from the LV apex or free wall, whereas the right ventricular free wall and outflow tract should be avoided. Transvenous leads may still be placed in the right ventricular apex given that it had the least negative hemodynamic influence of all right ventricular pacing sites. These patients, however, should be monitored for changes in ventricular performance. The mentioned principles may be applied to all children with a systemic LV and either spontaneous or surgical atrioventricular block. Care should be taken to place the leads at the LV apex rather than the LV base because the inverse pattern of electromechanical dyssynchrony caused by LV basal pacing might be detrimental in the long term. Given the fast developments in pacemaker technology and the expected introduction of leadless pacing systems with a potential for an easy application of LV pacing, our findings may also have importance for the future strategy of pacemaker therapy in adults.